



Studying Soft Interfaces with Shear Waves: Principles and Applications of the Quartz Crystal Microbalance (QCM-D)

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Principles and Applications of the Quartz Crystal Microbalance (QCM).

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<https://www.pc.tu-clausthal.de/en/research/qcm-modelling/>

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- Clausthal Group
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- **Andreas Böttcher**: Hardware
- **Philipp Sievers**: Software

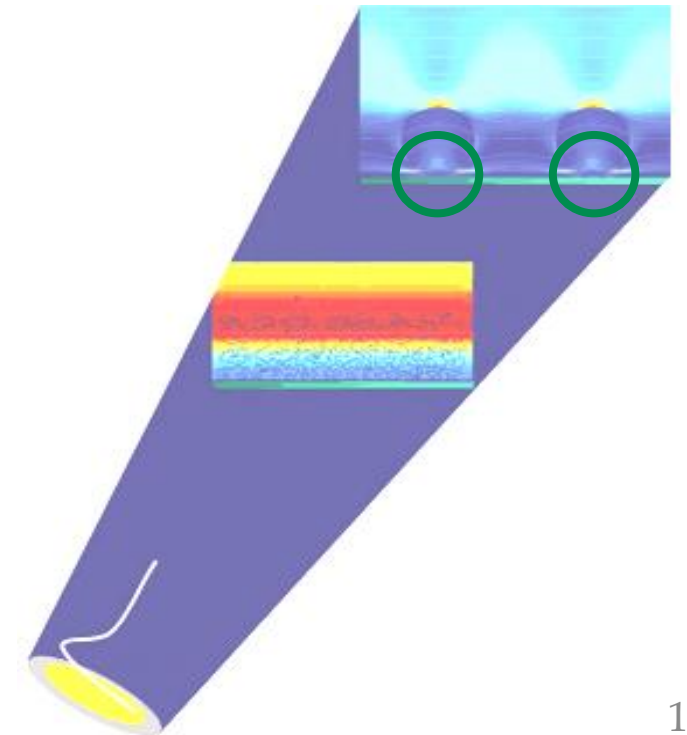
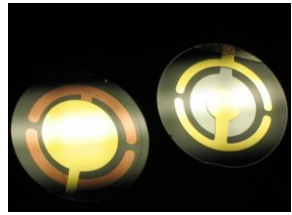
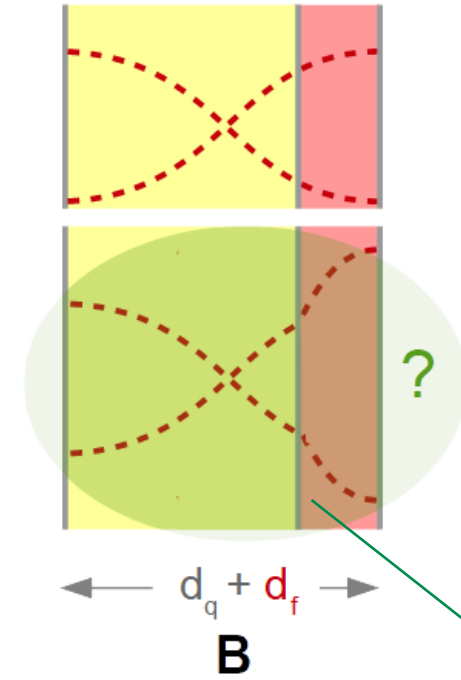
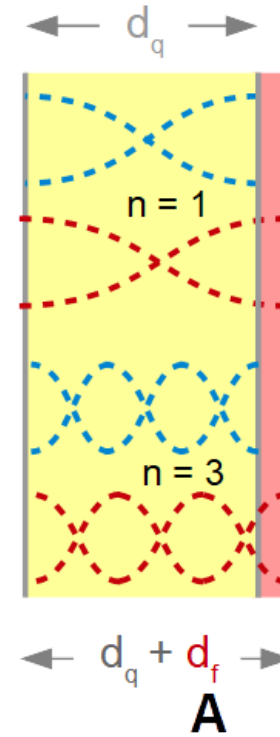
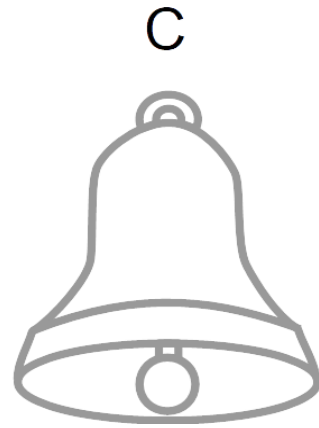
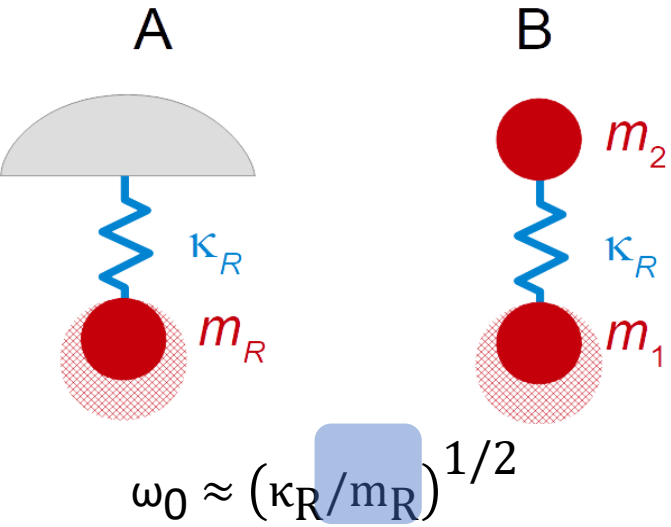


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 - thin films in a liquid
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 - software: QTM
-
- particles: positive Δf
 - fast measurements, applied to the electrochemical QCM

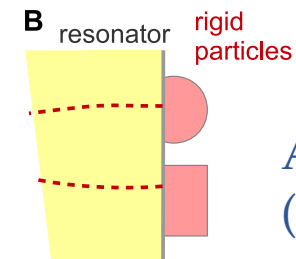
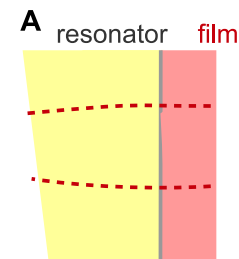
The QCM as a Gravimetric Sensor



$$\frac{\Delta f}{f_{ref}} = -\frac{m_f}{m_q}$$

$$\Delta f = -\frac{2nf_0^2}{Z_q} m_f$$

Sauerbrey 1959



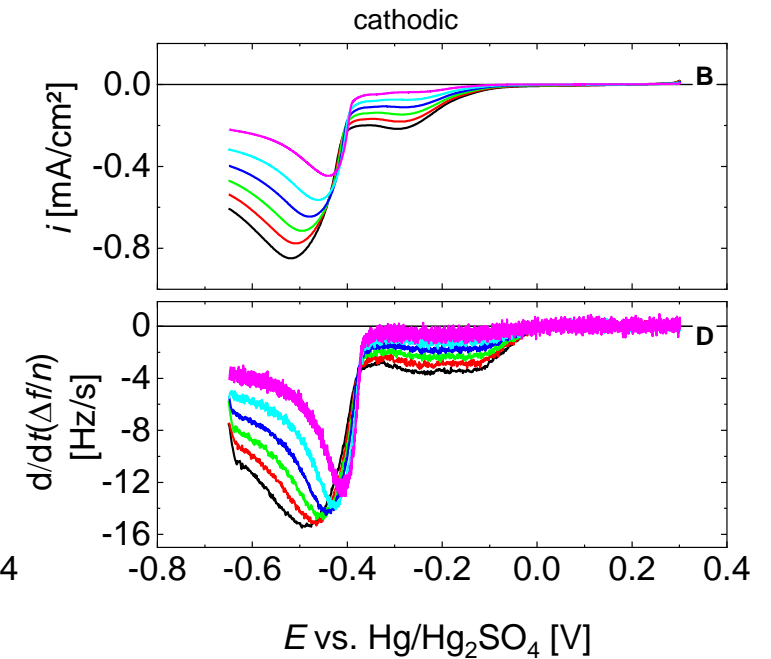
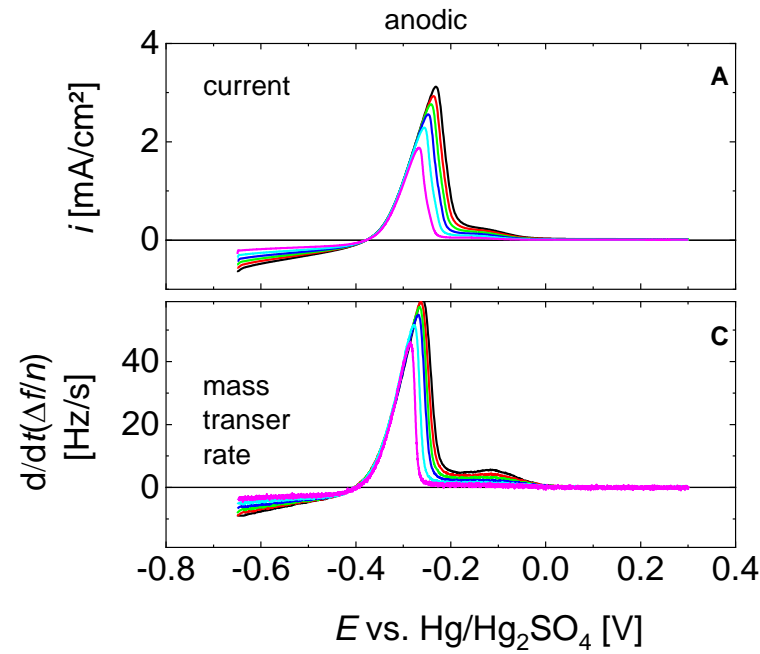
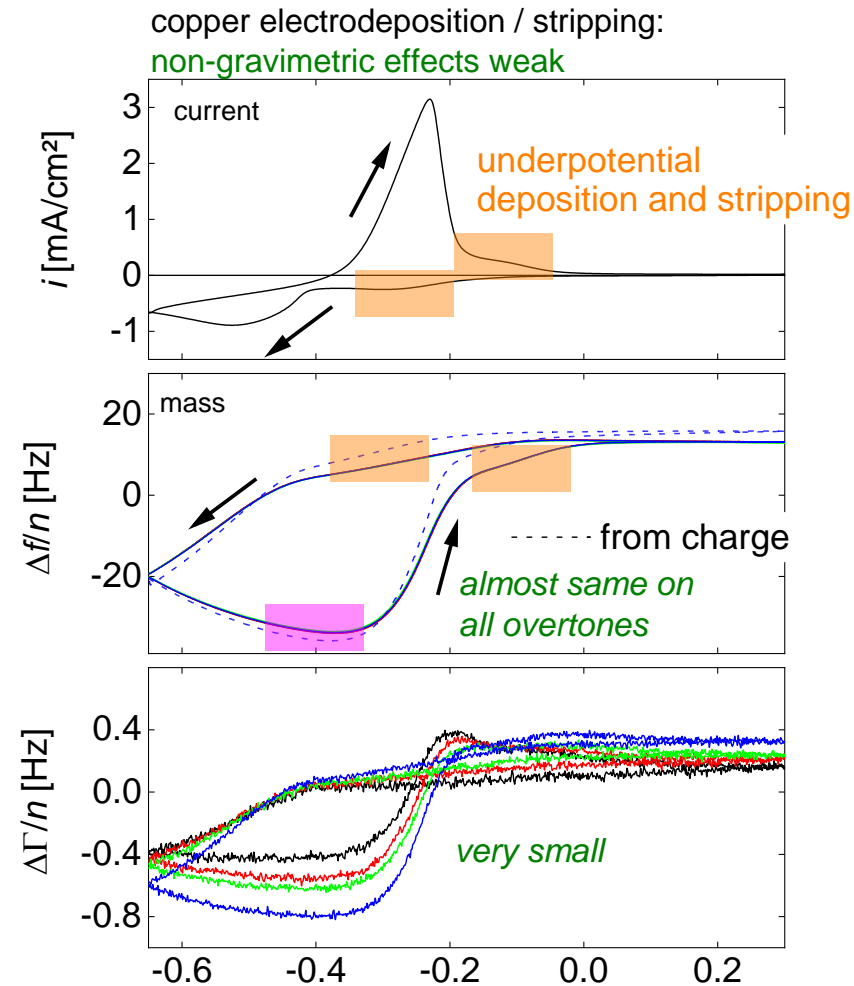
Also applies to
(small) particles

The QCM as a Gravimetric Sensor

Gravimetry not outdated

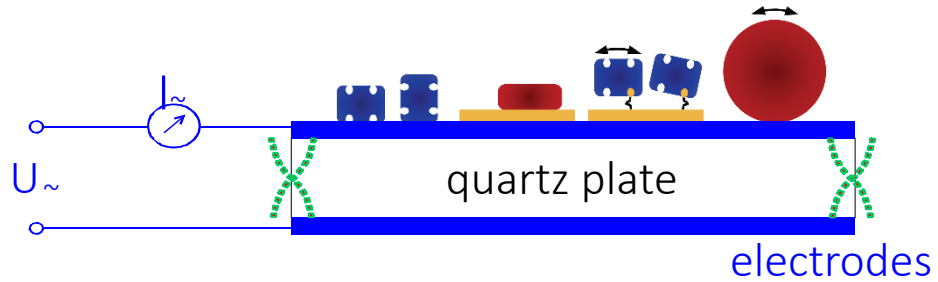
An example: Electrochemical QCM

current and mass-transfer rate are similar
... but not strictly the same

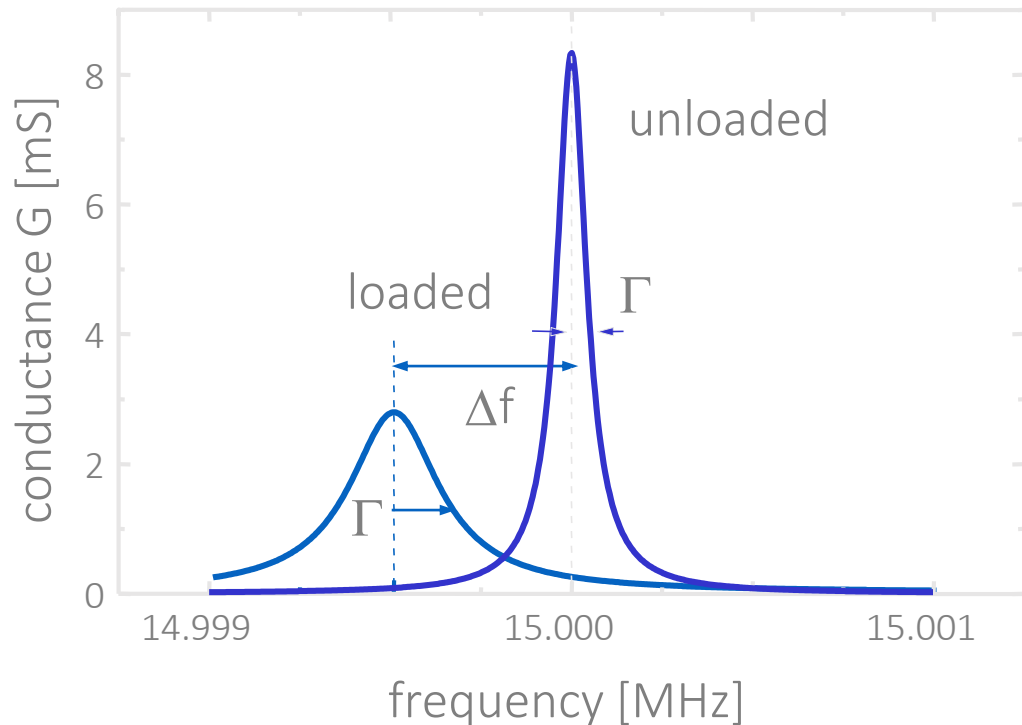


— 120 mV/s — 100 mV/s — 80 mV/s — 60 mV/s — 40 mV/s — 20 mV/s

Beyond Gravimetry: the QCM-D

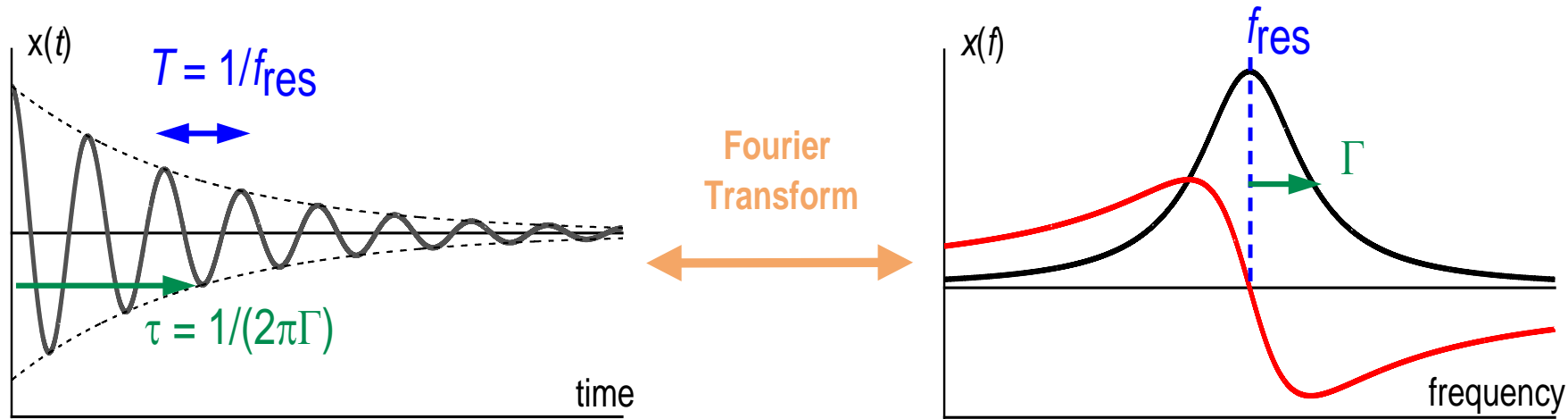


$f = f_{\text{res}}$: large amplitude of motion
 \Rightarrow large current



- Shifts in frequency and **bandwidth**: Δf , $\Delta\Gamma$
 Γ : half-band half width
 $\Delta\Gamma = \Delta D f_{\text{res}} / 2$
 ΔD : shift in dissipation factor, $D = Q^{-1}$
- Many **overtones** (5, 15, 25, 35, 45, 55, 65 MHz)
 $\Delta f(n)$, $\Delta\Gamma(n)$

Impedance Analysis and Ring-Down are Equivalent

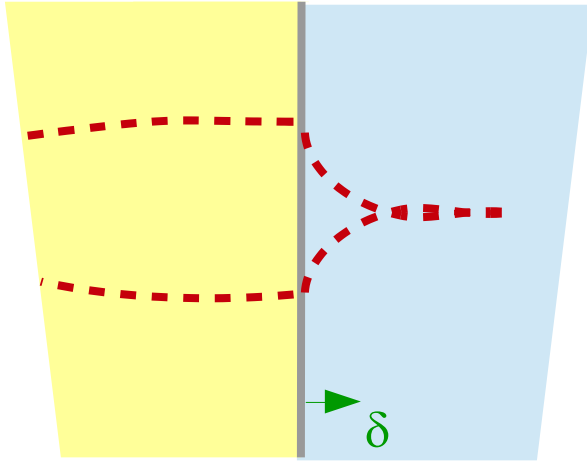


Ring-Down

Impedance Analysis

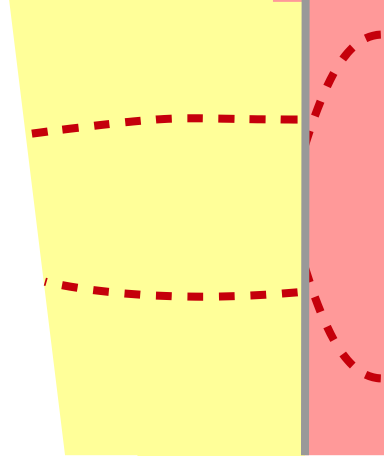
Three Important Cases

A resonator liquid



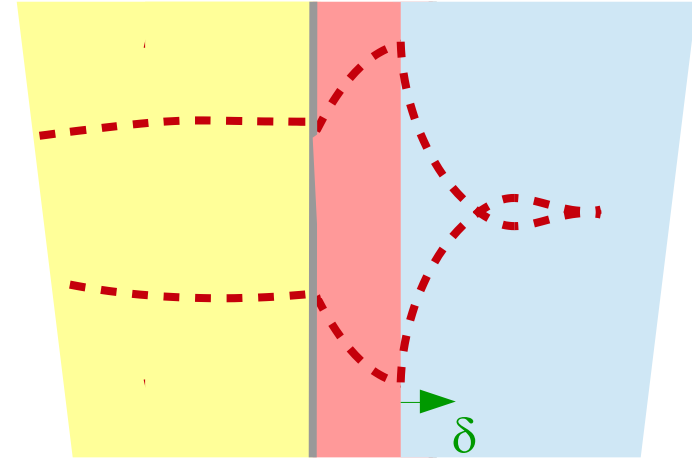
$$\frac{\Delta f + i\Delta\Gamma}{f_0} = \frac{i}{\pi Z_q} \sqrt{i\omega\rho\tilde{\eta}}$$

B resonator film



$$\frac{\Delta f + i\Delta\Gamma}{f_0} = \frac{i}{\pi Z_q} i\tilde{Z}_f \tan(\tilde{k}_f d_f)$$

C resonator film liquid



$$\frac{\Delta f + i\Delta\Gamma}{f_0} = \frac{-\tilde{Z}_f}{\pi Z_q} \cdot \frac{\tilde{Z}_f \tan(\tilde{k}_f d_f) - i\tilde{Z}_{\text{bulk}}}{\tilde{Z}_f + i\tilde{Z}_{\text{bulk}} \tan(\tilde{k}_f d_f)}$$

“ $\tilde{\quad}$ ”: complex variable

Structured Samples

Molecular Assemblies



Cells, Bacteria



???

Soft Layers



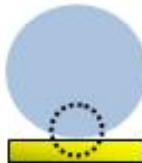
Materials



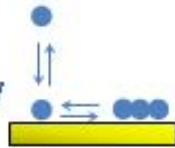
Atoms, Molecules



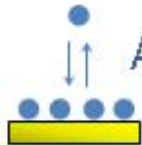
Contact Mechanics

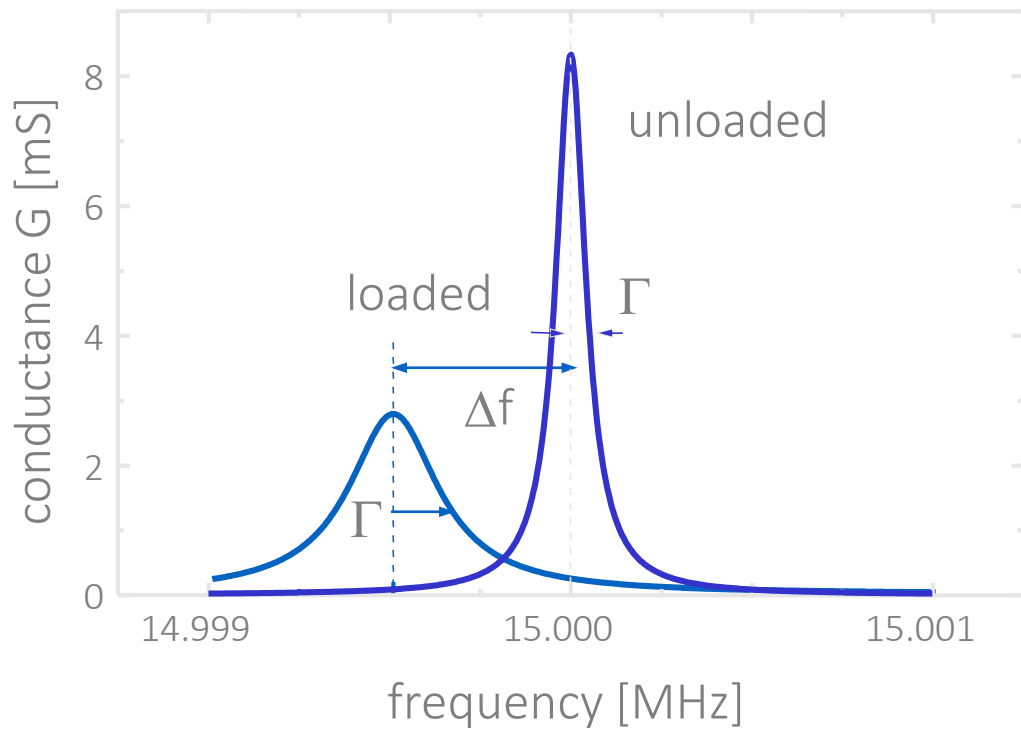


Biophysics, Pharmacology



Adsorption





The Small-Load Approximation

$$\frac{\Delta \tilde{f}}{f_0} = \frac{\Delta f + i\Delta\Gamma}{f_0} \approx \frac{i}{\pi Z_q} \tilde{Z}_L = \frac{i}{\pi Z_q} \frac{\hat{\sigma}}{\hat{v}}$$

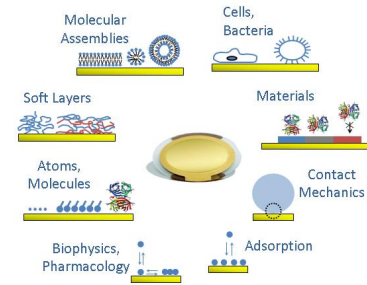
$$\tilde{Z}_L = \frac{\hat{\sigma}}{\hat{v}} \text{ "load impedance",}$$

can be **area - averaged** $\tilde{Z}_L \rightarrow \langle \tilde{Z}_L \rangle_{\text{area}}$

$\hat{\sigma}$ stress

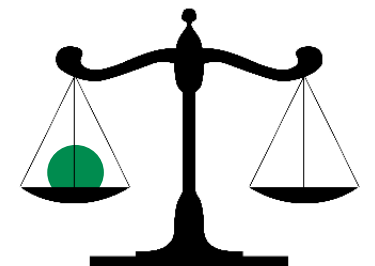
\hat{v} velocity

$\hat{\cdot}$: complex amplitude ($\sigma(t) = \hat{\sigma} \exp(i\omega t)$)



QCM: The Quartz Crystal Micro *Stress*-Balance

- periodic stress,
- in-phase and out-of-phase component determined separately



Semi-Infinite Liquids

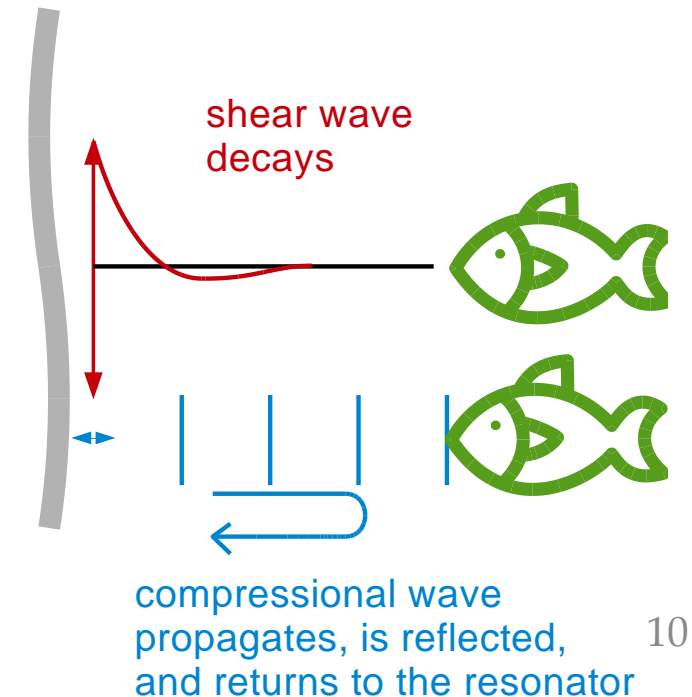
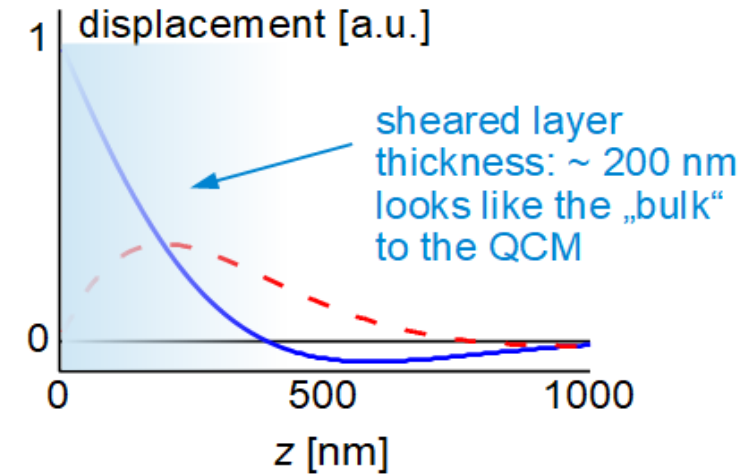
- finite depth of penetration $\delta = (2\eta/(\rho\omega))^{1/2} \approx 200$ nm
 → QCM is **surface specific**
 unless... compressional waves are reflected somewhere.
 Avoid a geometry, where the opposite cell wall is parallel to the sensor surface.

- the load impedance is equal to the liquid's shear-wave impedance $\tilde{Z}_L = \tilde{Z}_{\text{bulk}} = \sqrt{\rho\tilde{G}} = \sqrt{\rho i\omega\tilde{\eta}}$
 → **Gordon-Kanazawa**

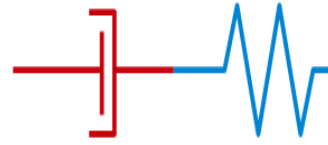
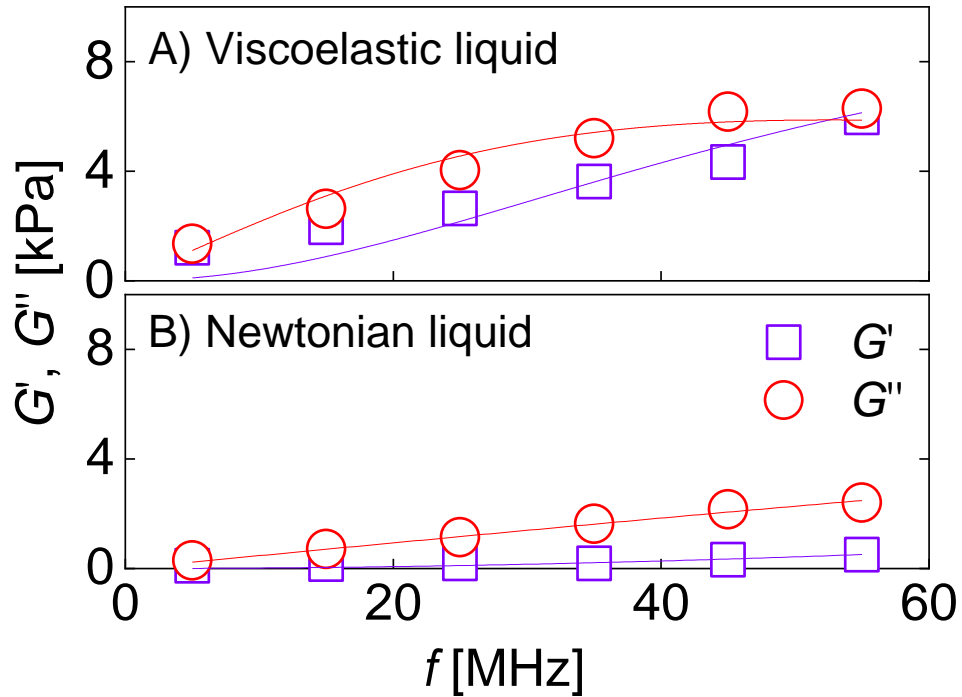
$$\frac{\Delta f + i\Delta\Gamma}{f_0} = \frac{i}{\pi Z_q} \tilde{Z}_{\text{bulk}} = \frac{-1+i}{\sqrt{2}} \frac{1}{\pi Z_q} \sqrt{\omega\rho(\eta' - i\eta'')}$$

$$\varrho\eta' = \frac{G''}{\omega} = -\frac{\pi Z_q^2}{f_{\text{res}}^2} \frac{1}{2} \frac{\Delta f \Delta\Gamma}{f_0^2}$$

$$\varrho\eta'' = \frac{G'}{\omega} = \frac{\pi Z_q^2}{f_{\text{res}}^2} \frac{(\Delta\Gamma^2 - \Delta f^2)}{f_0^2}$$



Viscoelastic Semi-Infinite Liquids



$$i\omega(\eta' - i\eta'')$$

$$= G' + iG''$$

$$= G_\infty / (1 - i\omega\tau)$$

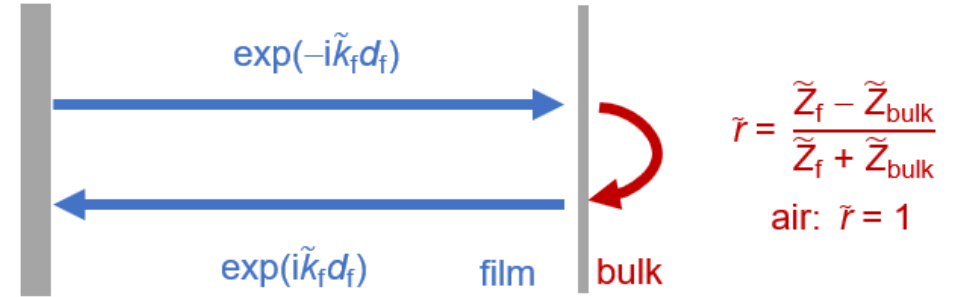
τ : relaxation time



Hartl, J.; Peschel, A.; Johannsmann, D.; Garidel, P. Characterizing protein-protein-interaction in **high-concentration monoclonal antibody systems** with the quartz crystal microbalance.

Phys. Chem. Chem. Phys. 2017, 19, 32698

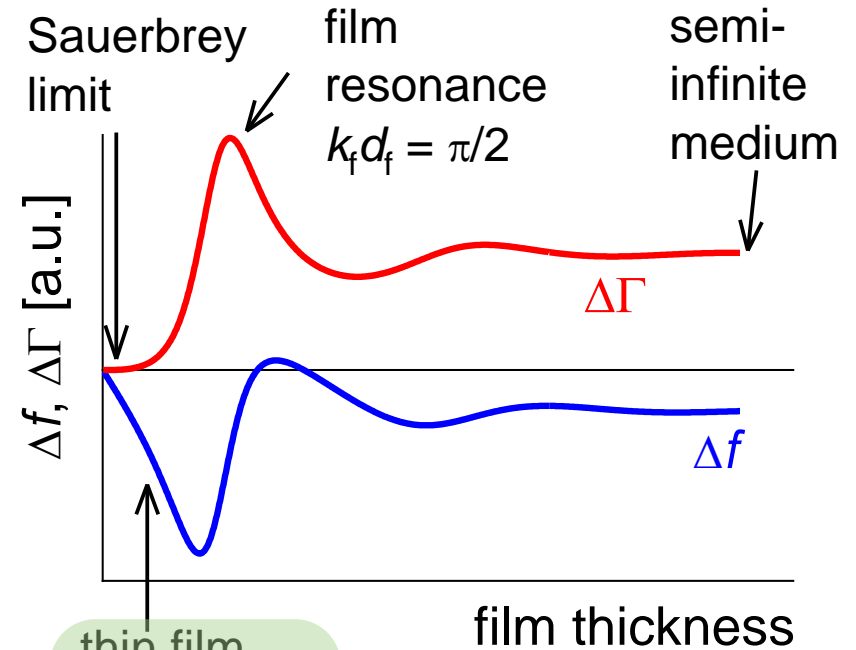
Film in Air



$$\tilde{Z}_L = \tilde{Z}_f \frac{\hat{v}_{\rightarrow} - \hat{v}_{\leftarrow}}{\hat{v}_{\rightarrow} + \hat{v}_{\leftarrow}} = \tilde{Z}_f \frac{1 - \frac{\hat{v}_{\leftarrow}}{\hat{v}_{\rightarrow}}}{1 + \frac{\hat{v}_{\leftarrow}}{\hat{v}_{\rightarrow}}} = \tilde{Z}_f \frac{1 - \tilde{r}_S}{1 + \tilde{r}_S}$$



$$\frac{\Delta f + i\Delta\Gamma}{f_0} = \frac{i}{\pi Z_q} i\tilde{Z}_f \tan(\tilde{k}_f d_f)$$



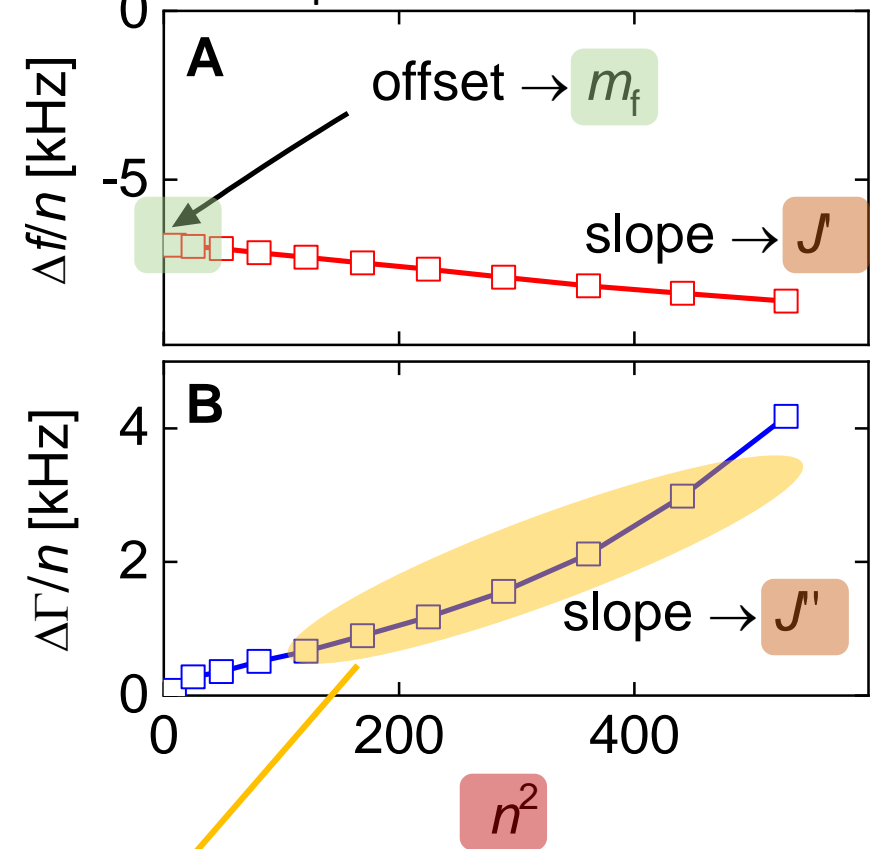
Thin Film in Air

$$\frac{\Delta f + i\Delta\Gamma}{f_0} \approx -\frac{\omega m_f}{\pi Z_q} \left[1 + \frac{(n\pi)^2}{3} \left(\frac{\tilde{J}_f}{\rho_f} Z_q^2 - 1 \right) \left(\frac{m_f}{m_q} \right)^2 \right]$$

- prefactor: **gravimetric**
- second term in square brackets: **viscoelastic correction**
 $\propto m_f^2$ because film shears under its own inertia,
 viscoelastic effects only seen if $d_f > 100$ nm
 $\propto n^2$
 depends on $\tilde{J}_f = J' - iJ''$: viscoelastic compliance
 $\tilde{J}_f = (\tilde{G}_f)^{-1} = (G' + iG'')^{-1}$, \tilde{G} : shear modulus

The non-trivial samples are the **soft** samples

spin-cast film of polyisopropylene,
 $\sim 1.7 \mu\text{m}$ thick



Domack, A.; Johannsmann, D.,
 Plastification during sorption of polymeric thin films: A quartz resonator study.
Journal of Applied Physics 1996, 80, (5), 2599.

$$G' = \frac{J'}{J'^2 + J''^2}, \quad G'' = \frac{J''}{J'^2 + J''^2}$$

Viscoelastic Dispersion

Soft samples: **stress relaxation** on the time scale of f_{res}^{-1}

$$\rightarrow \tilde{J}_f = \tilde{J}_f(\omega)$$

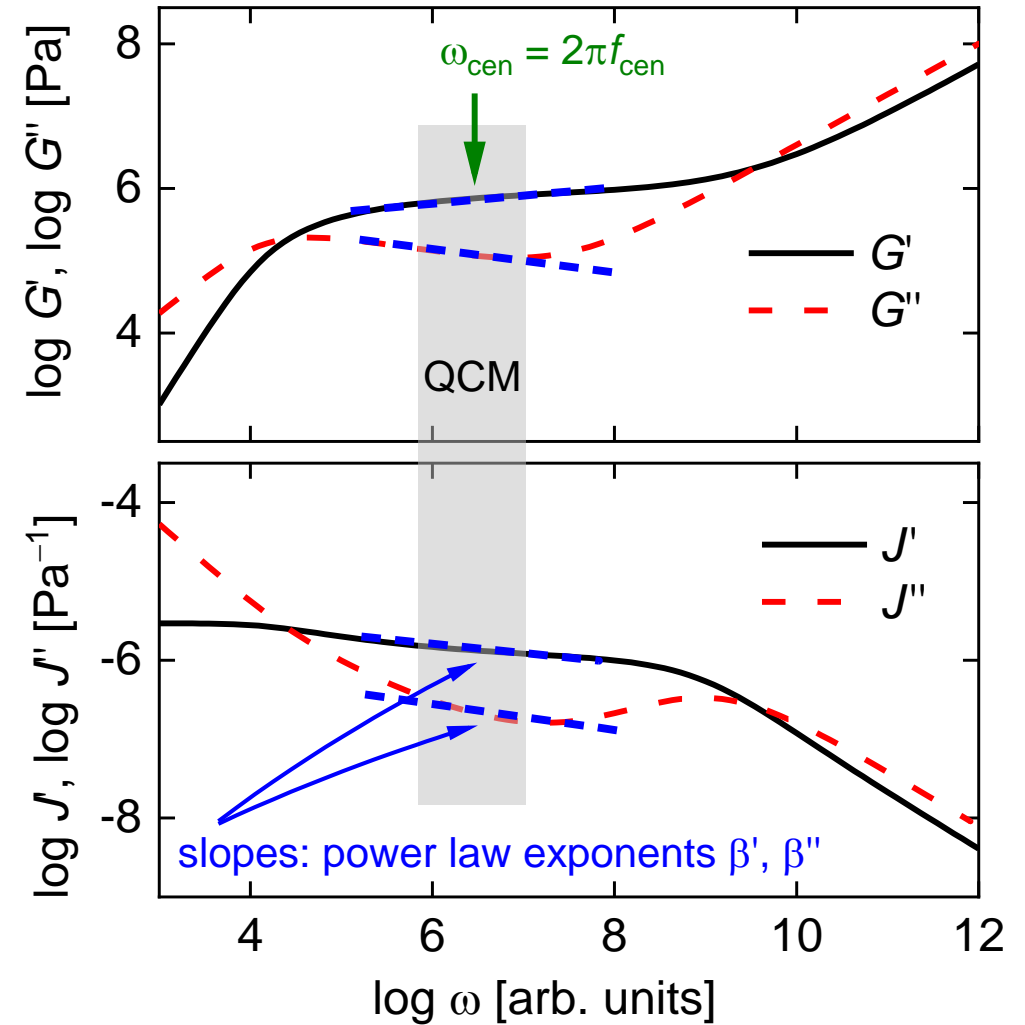
Viscoelastic spectra are smooth.

In the frequency range covered by the QCM, they can be approximated by **power laws**.

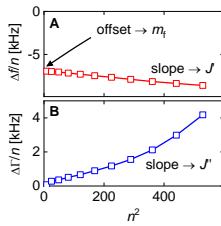
$$J_f'(f) \approx J_f'(f_{\text{cen}}) \left(\frac{f}{f_{\text{cen}}} \right)^{\beta'}$$

$$J_f''(f) \approx J_f''(f_{\text{cen}}) \left(\frac{f}{f_{\text{cen}}} \right)^{\beta''}$$

The 5 fit parameters are $d_f, J_f'(f_{\text{cen}}), J_f''(f_{\text{cen}}), \beta', \beta''$



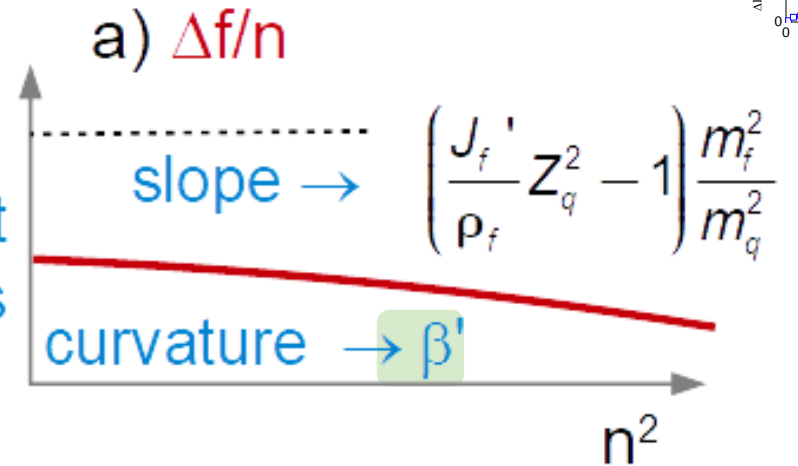
$\Delta\Gamma/(-\Delta f)$



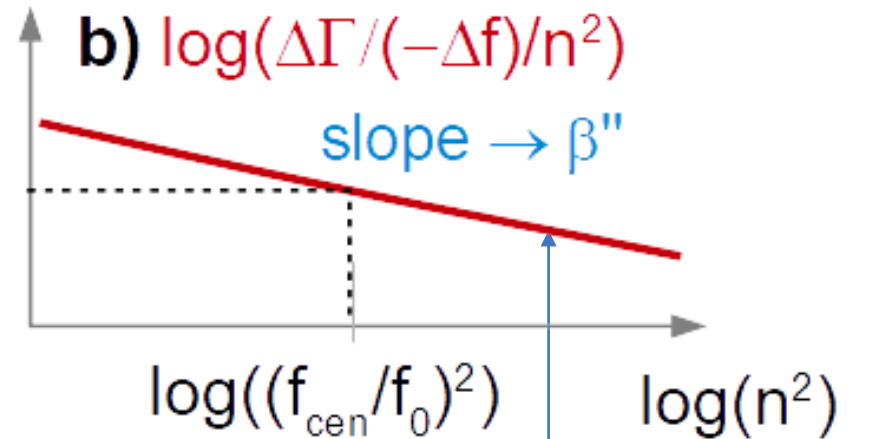
$$\frac{\Delta f + i\Delta\Gamma}{f_0} \approx -\frac{\omega m_f}{\pi Z_q} \left[1 + \frac{(n\pi)^2}{3} \left(\frac{\tilde{J}_f}{Q_f} Z_q^2 - 1 \right) \left(\frac{m_f}{m_q} \right)^2 \right]$$

$$\frac{\Delta\Gamma}{-\Delta f} \approx \frac{(n\pi)^2}{3} \left(\frac{J''_f(\omega)}{Q_f} Z_q^2 \right) \left(\frac{m_f}{m_q} \right)^2$$

intercept
→ thickness



→ J''



β' ← curvature in $\Delta f/n$ vs n ,
often not determined with sufficient accuracy ☹

The 4 fit parameters determined with confidence are
 $d_f, J'_f(f_{\text{cen}}), J''_f(f_{\text{cen}}), \beta', \beta''$

$$J''_f(f) \approx J''_f(f_{\text{cen}}) \left(\frac{f}{f_{\text{cen}}} \right)^{\beta''}$$

Thin Film in Liquid (*different from film in air*)

$$\frac{\Delta f + i\Delta\Gamma}{f_0} = - \frac{\omega m_f}{\pi Z_q} \left[1 - \frac{\tilde{J}_f(\omega)}{\rho_f} i\omega \rho_{\text{bulk}} \eta_{\text{bulk}} \right]$$

$$\frac{\Delta f}{n} + i \frac{\Delta\Gamma}{n} \approx - \frac{2f_0^2}{Z_q} m_f \left[1 - n \left(J_f'(\omega) - iJ_f''(\omega) \right) \left(2\pi i f_0 \frac{\rho_{\text{bulk}}}{\rho_f} \eta_{\text{bulk}} \right) \right]$$

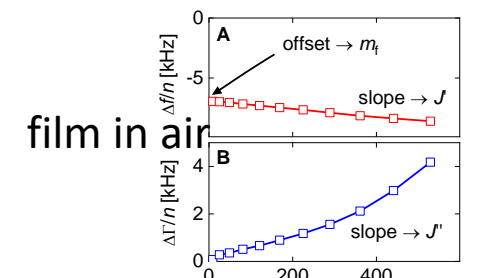
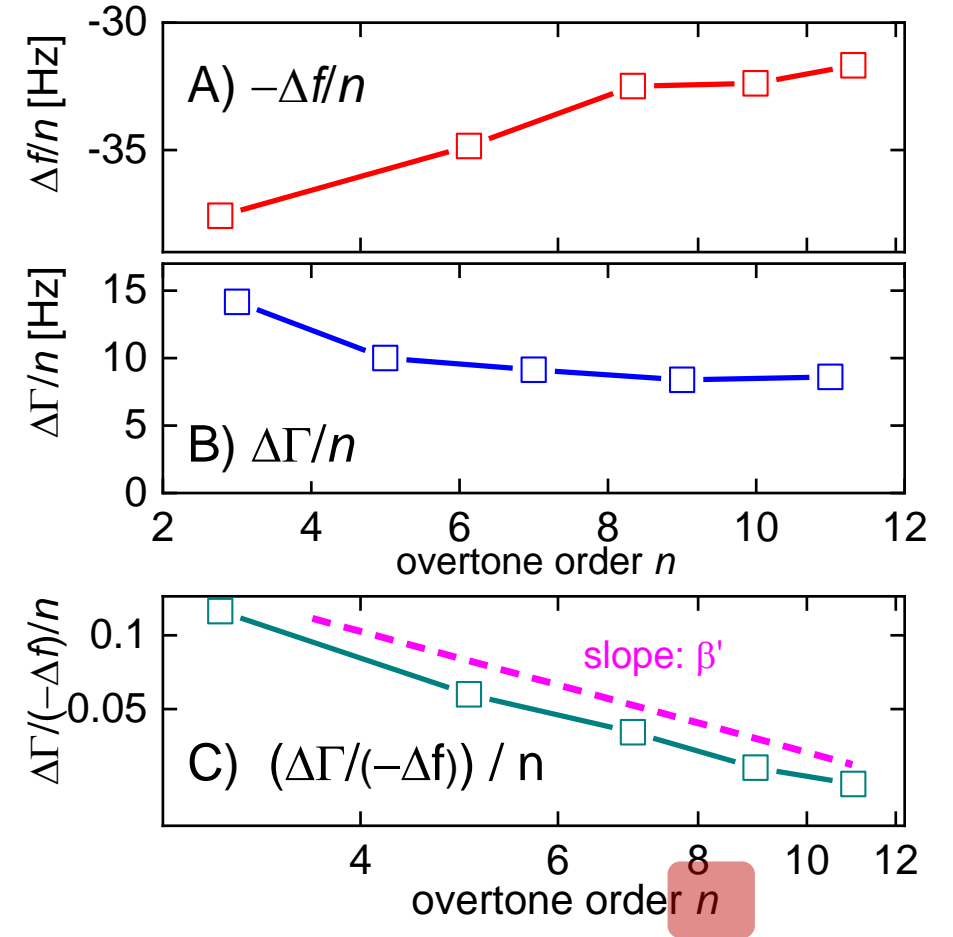
prefactor: gravimetric

second term in square brackets: viscoelastic correction

- $\propto \eta_{\text{bulk}}$ because film shears under the stress exerted by the bulk

viscoelastic effects seen even for protein monolayers

- $\propto n$
- is negative (*lowers* the apparent mass, „missing mass effect“)



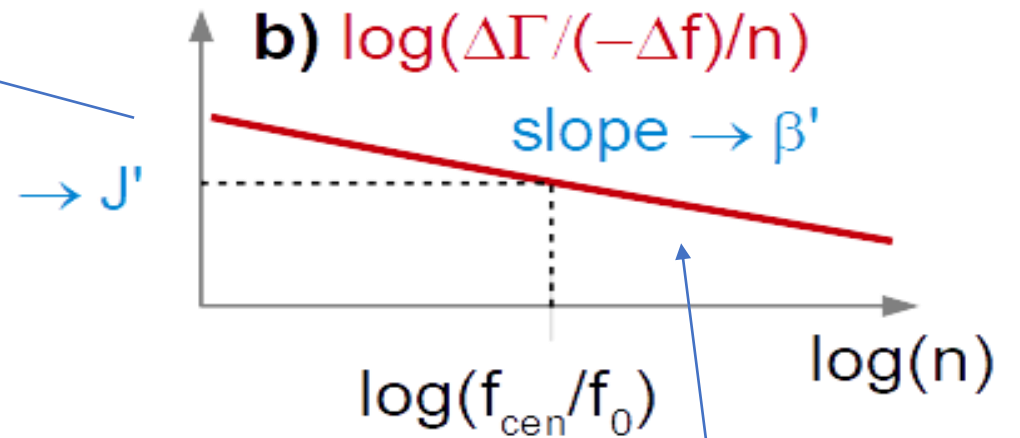
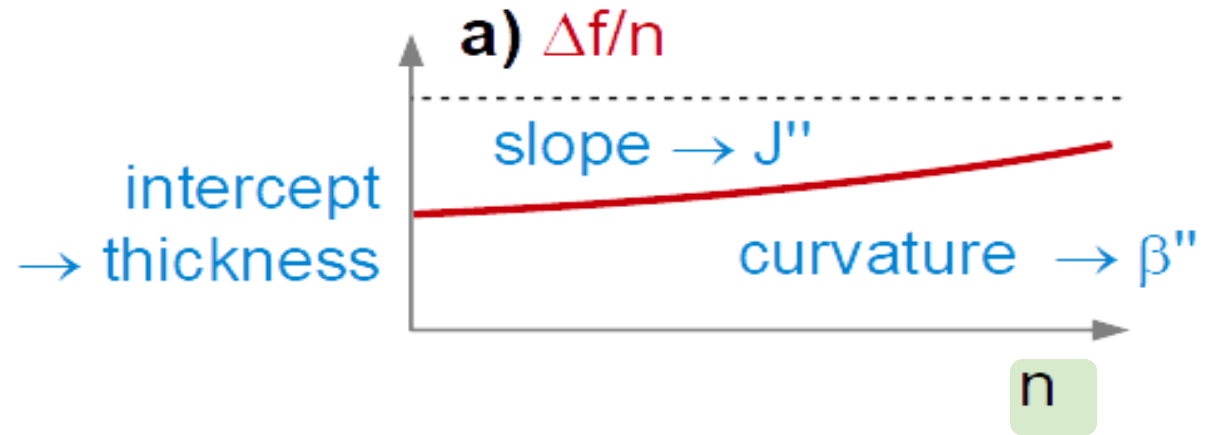
$$\frac{\Delta\Gamma}{(-\Delta f)}$$

$$\frac{\Delta\Gamma}{-\Delta f} \approx n J_f'(\omega) 2\pi f_0 \eta_{\text{bulk}}$$

$\beta'' \leftarrow$ curvature in $\Delta f/n$ vs n ,
often not determined with sufficient accuracy ☹

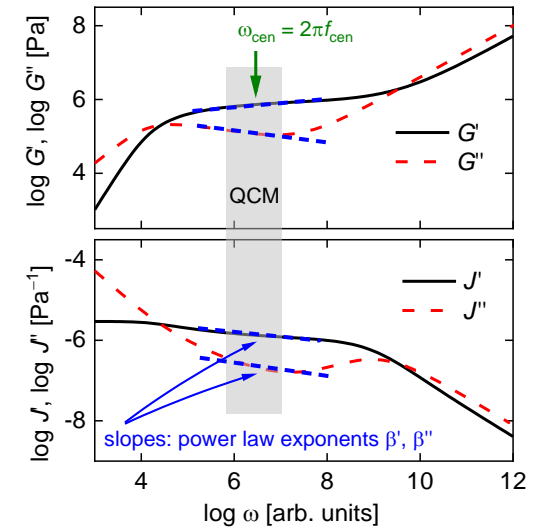
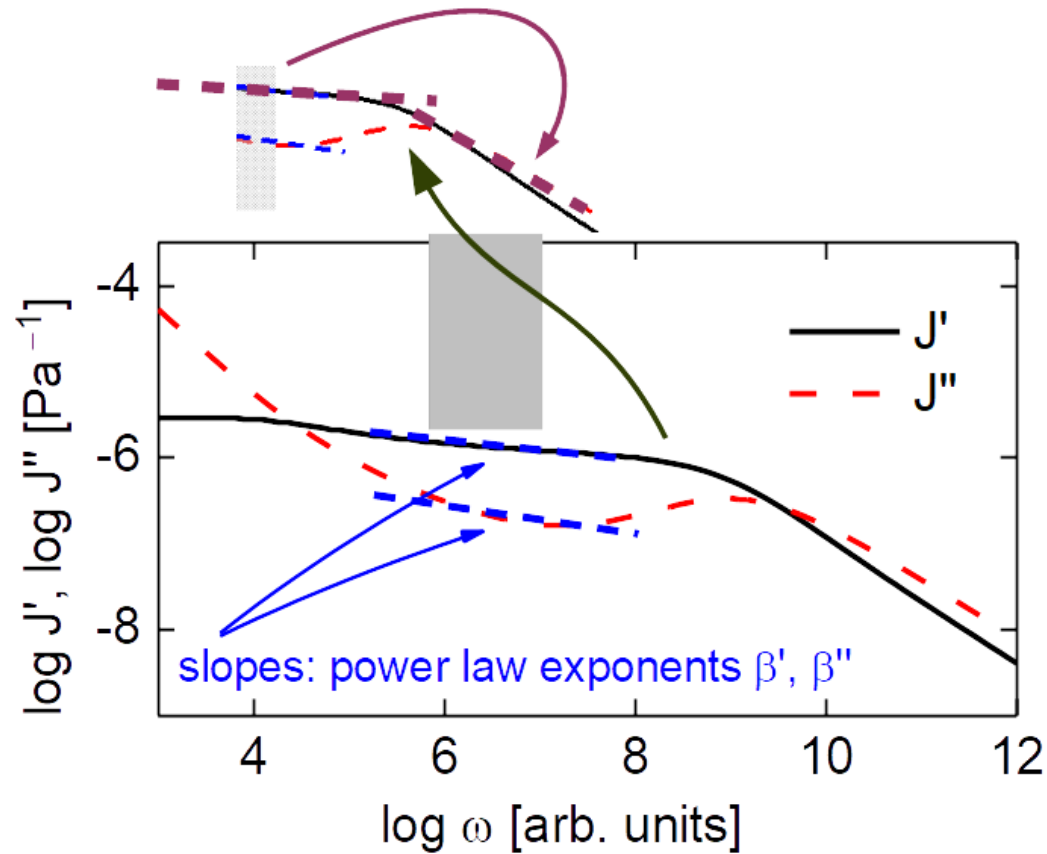
The 4 fit parameters determined with confidence
are $d_f, J_f'(f_{\text{cen}}), J_f''(f_{\text{cen}}), \beta', \beta''$

Note the differences between the film in air
and the film in a liquid.



$$J_f'(f) \approx J_f'(f_{\text{cen}}) \left(\frac{f}{f_{\text{cen}}} \right)^{\beta'}$$

Interpretation of β'



In this example, a decrease in β' (to more negative values) is indicative of a decreased rate of relaxation.

This argument requires an assumption on the function $\tilde{J}(\omega)$

Polymer Brushes, Samples with Viscoelastic Profiles

$$m_f \rightarrow m_{\text{app}}$$

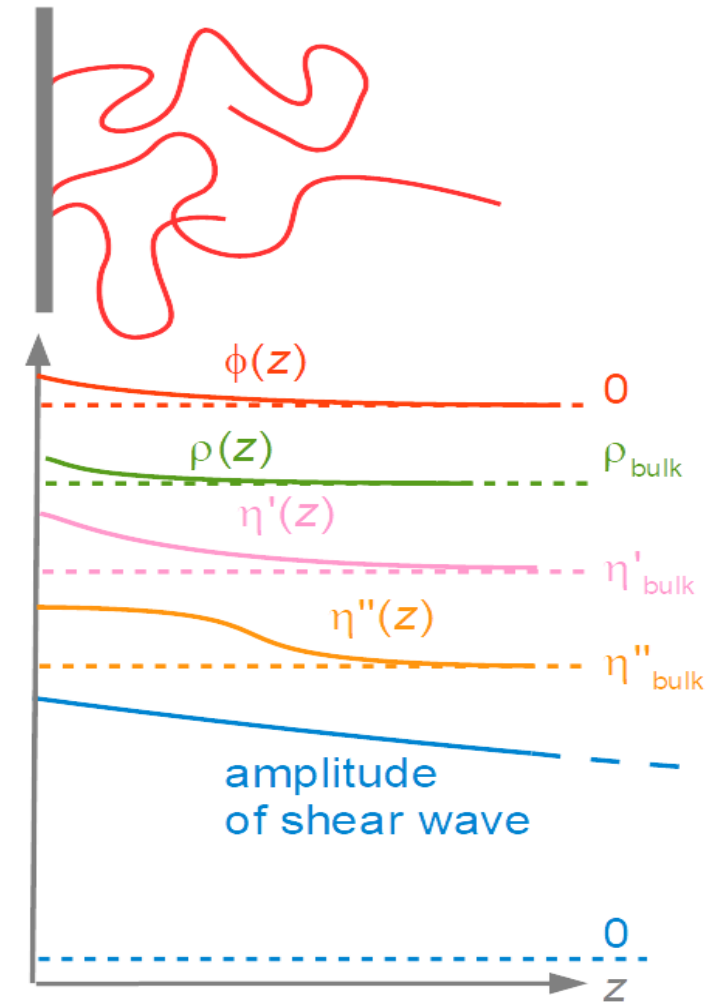
$$J'_f \rightarrow J'_{\text{app}}$$

$$\tilde{m}_{\text{app}}(n) = \frac{Zq}{2nf_0^2} \Delta \tilde{f}(n) \approx \int_0^\infty \rho_{\text{bulk}} \left[\frac{\rho(z)}{\rho_{\text{bulk}}} - \frac{\eta_{\text{bulk}}}{\tilde{\eta}(n,z)} \right] dz$$

$$J_{\text{app}}'(n) = \frac{\Delta \Gamma}{-\Delta f \omega \eta_{\text{bulk}}} \frac{1}{\int_0^\infty (1 - \omega \eta_{\text{bulk}} J''(z)) \rho(z) dz} \int_0^\infty J'(z) \rho(z) dz$$

$$\approx \frac{\rho_{\text{bulk}}}{m'_{\text{app}}} \int_0^\infty J'(z) dz$$

A word of caution: Interpretation is robust for thin layers. For thicker layers (> 100 nm), the acoustic waves have trouble distinguishing between a thick, dilute layer and thin, more compact layer. ☹️



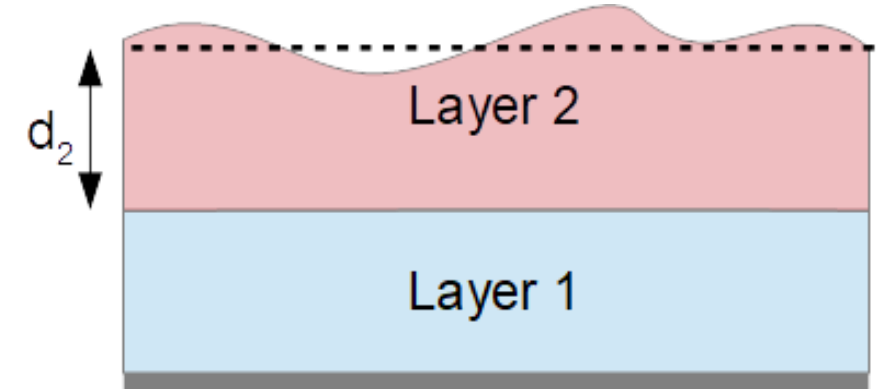
Small-Scale Roughness

$$\frac{\Delta f + i\Delta\Gamma}{f_0} = -\frac{1}{\pi Z_q} \omega \rho h_r \frac{3\sqrt{\pi} h_r}{2 l_r} + \frac{i}{\pi Z_q} \sqrt{i\omega \rho \eta} \left[1 - 2i \left(\frac{h_r}{\delta} \right)^2 \right]$$

- h_r : vertical scale of roughness (must be $\ll \delta$)
- l_r : lateral scale of roughness
- h_r/l_r : aspect ratio (must be $\ll 1$)

- in **green**: a gravimetric term (Sauerbrey-like, trapped mass), scales as h_r (as long as the aspect ratio is fixed)
- in **orange**: an effective bulk impedance of the liquid, change scales as h_r^2 , affects Δf and $\Delta\Gamma$ in a similar way

Small scale roughness affects Δf stronger than $\Delta\Gamma$.



The Software Package QTM

An adsorption experiment (BSA),
data from Ilya Reviakine

<https://www.pc.tu-clausthal.de/en/research/qcm-modelling/>

File Settings Model Limits Convert Exponents Df,dG vs act. par. chi²-Landscape Analyze Time Traces About

Thickness [nm] rho [g/cm³] J' [MPa⁻¹] PL.Exp. J' J'' [MPa⁻¹] PL.Exp. J''

1 9.041 1.000 0.24938 -0.911 0.33689 -0.500 J', J''

2

rho [g/cm³] eta' [mPa s] PL.Exp. J' eta'' [mPa s] PL.Exp. J''

Bulk Liquid 1.000 0.89000 0.000 0.00000 -1.000 eta', eta''

Model Pars

x10 /10
x5 /5
x2 /2
x1.5 /1.5
x1.1 /1.1
x1.01 /1.01
-> Reference

Fit <- Backup
4 Fit Parameters
 χ^2 0.61382
Weight ~ 1/n
Fit Df and DG

Experimental Data

Df/n [Hz], DD[10⁻⁶]

<- Clipboard Clear

| n | Df/n [Hz] | DD [10 ⁻⁶] |
|--|-----------|------------------------|
| <input type="checkbox"/> 1.0 | -50.48 | 0.83 |
| <input checked="" type="checkbox"/> 3.0 | -49.54 | 0.77 |
| <input checked="" type="checkbox"/> 5.0 | -48.17 | 1.05 |
| <input checked="" type="checkbox"/> 7.0 | -48.43 | 1.13 |
| <input checked="" type="checkbox"/> 9.0 | -47.74 | 1.23 |
| <input checked="" type="checkbox"/> 11.0 | -47.12 | 1.12 |
| <input type="checkbox"/> 13.0 | | |
| <input type="checkbox"/> 15.0 | | |
| <input type="checkbox"/> 17.0 | | |
| <input type="checkbox"/> 19.0 | | |

FitPars -> Clpbrd

Display y-axis Df/n, DDissipFact
Auto-Scale x x-axis n

Fundamental : 5.000 MHz Ref. Freq. VE Pars : 30.000 MHz Zq [10⁶ kg/(m² s)]: 8.80 AMF Ref: t_1 : 0.0 t_2 : 0.

933.662

Experiment AMF

Df/n [Hz]

Overtone Order n

Graph -> Clipboard

933.662

Experiment AMF

DDissfac [10⁻⁶]

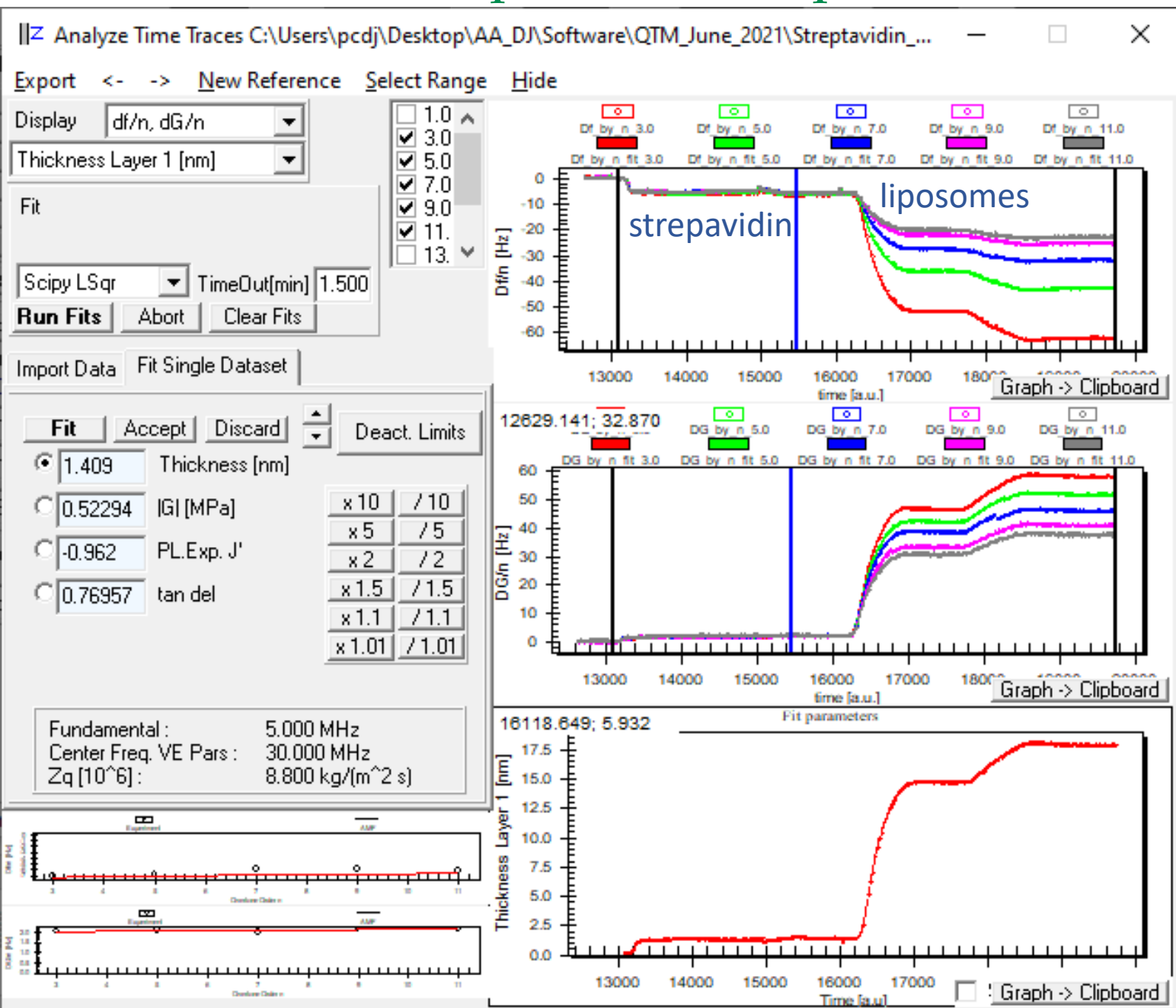
Overtone Order n

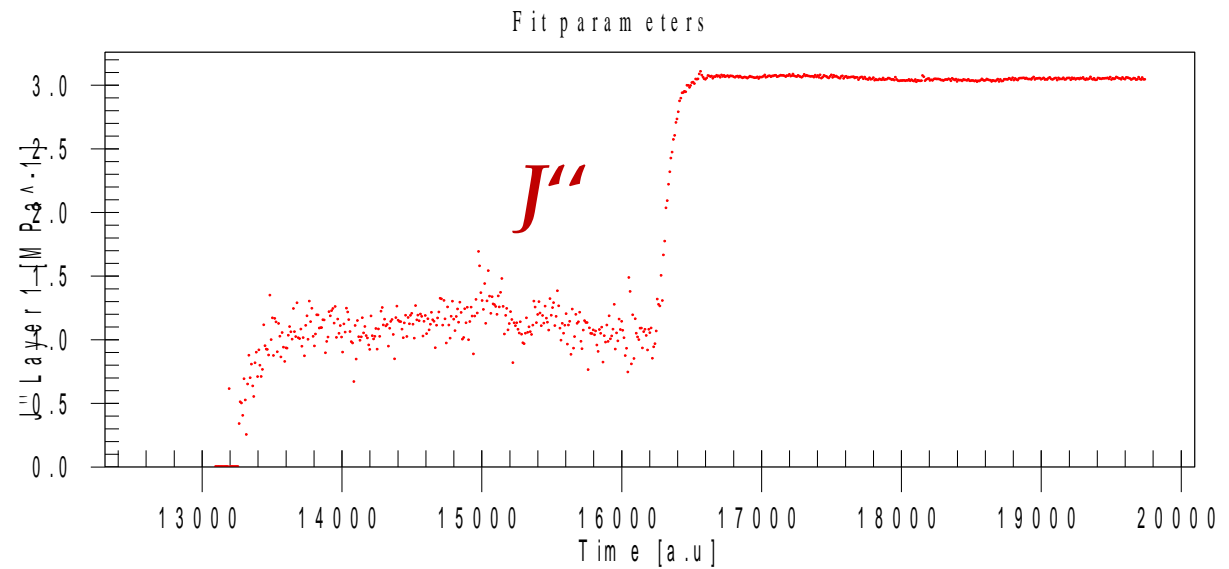
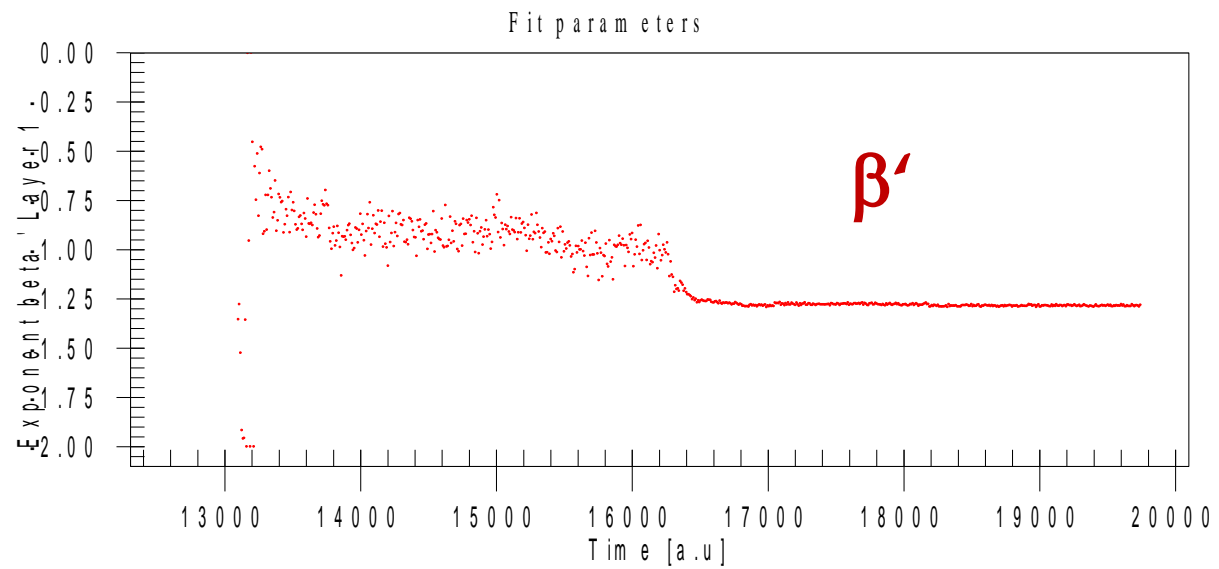
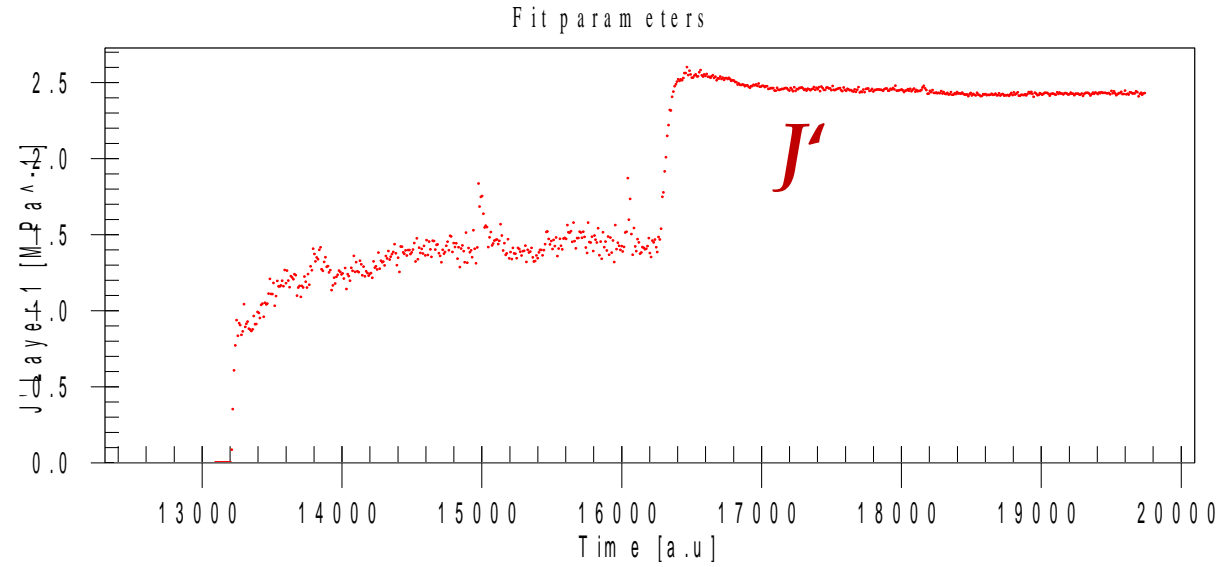
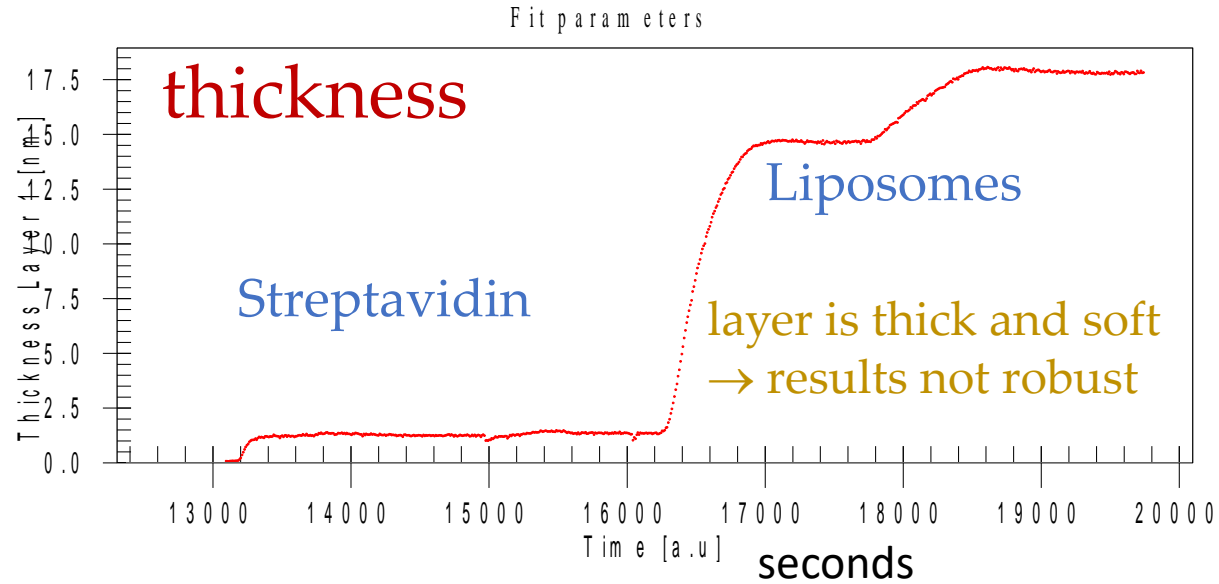
Graph -> Clipboard

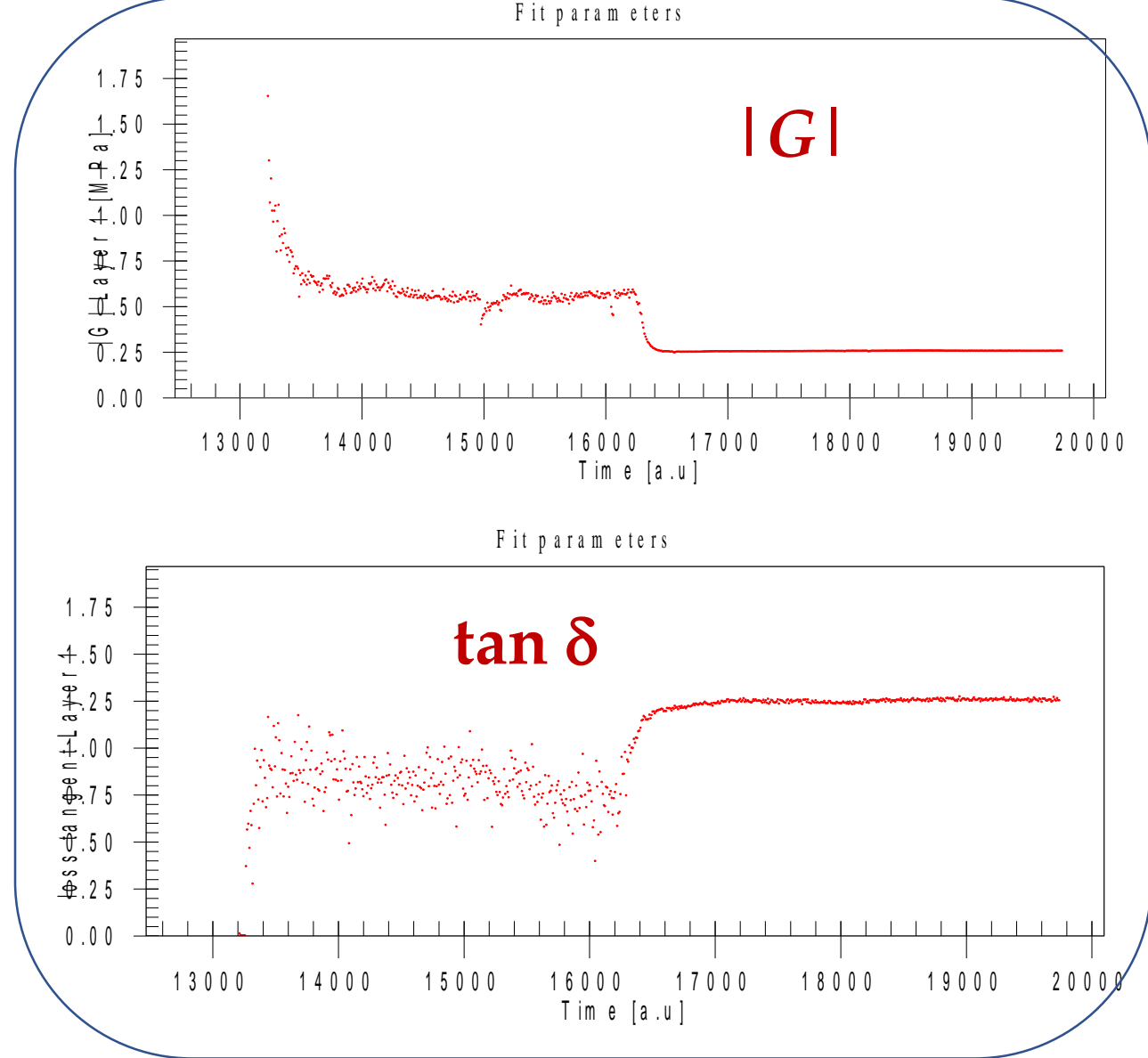
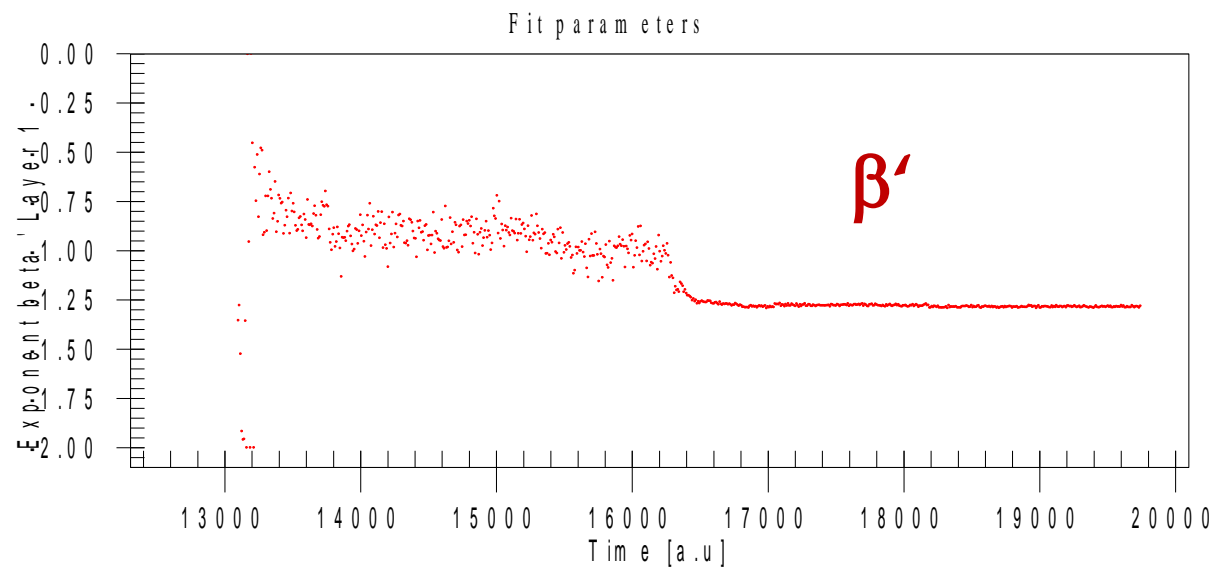
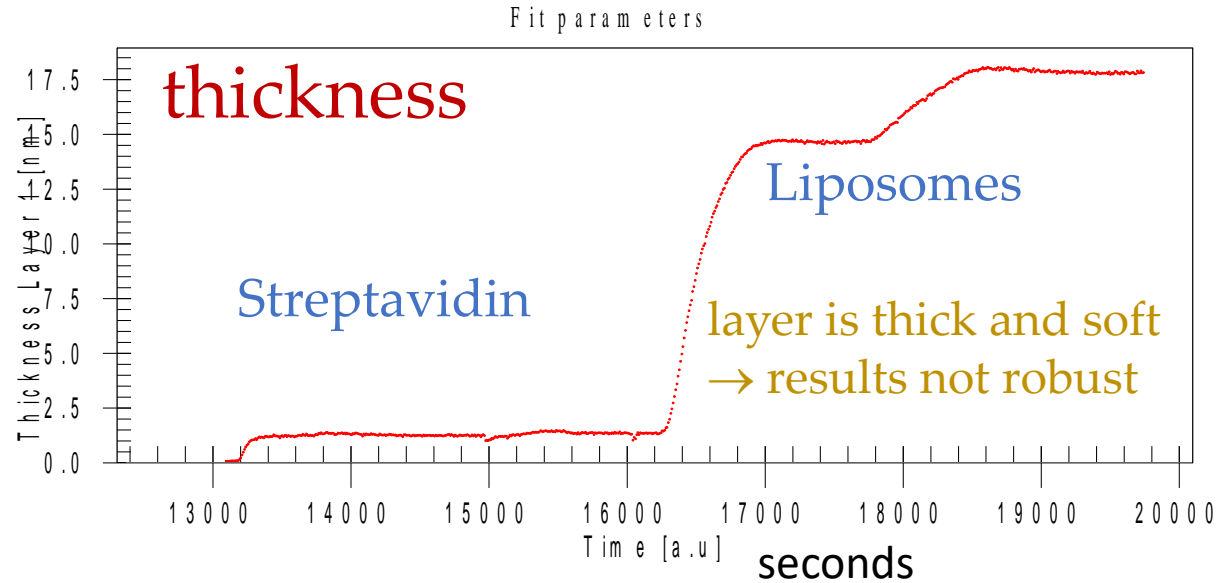
Those deviations are similar
over the entire experiment.
(this is not „noise“ in the
narrow sense)

Streptavidin + Liposomes

First streptavidin,
then liposomes,
data from Ilya Reviakine

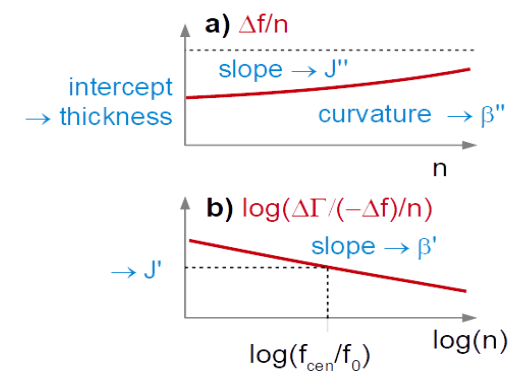
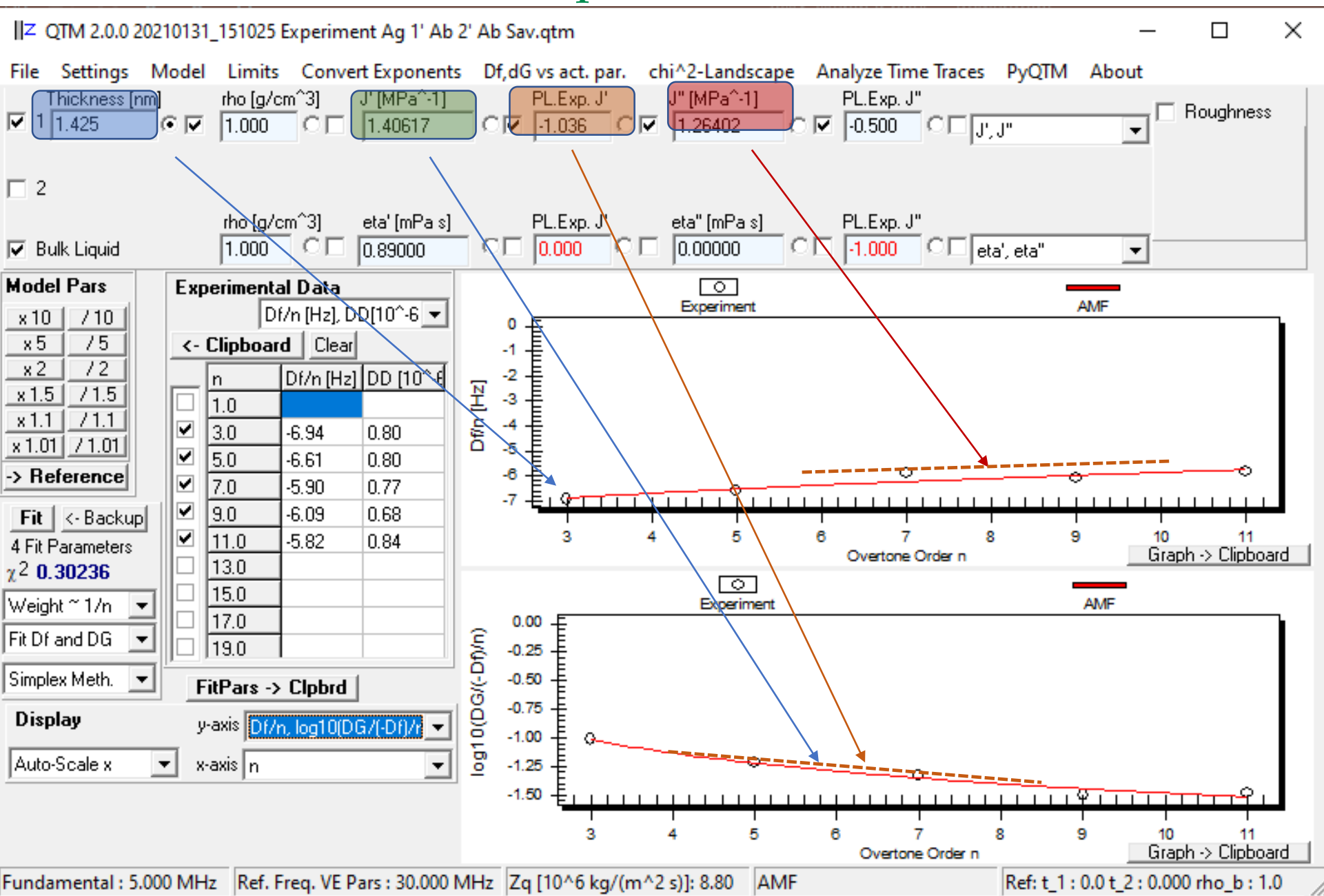






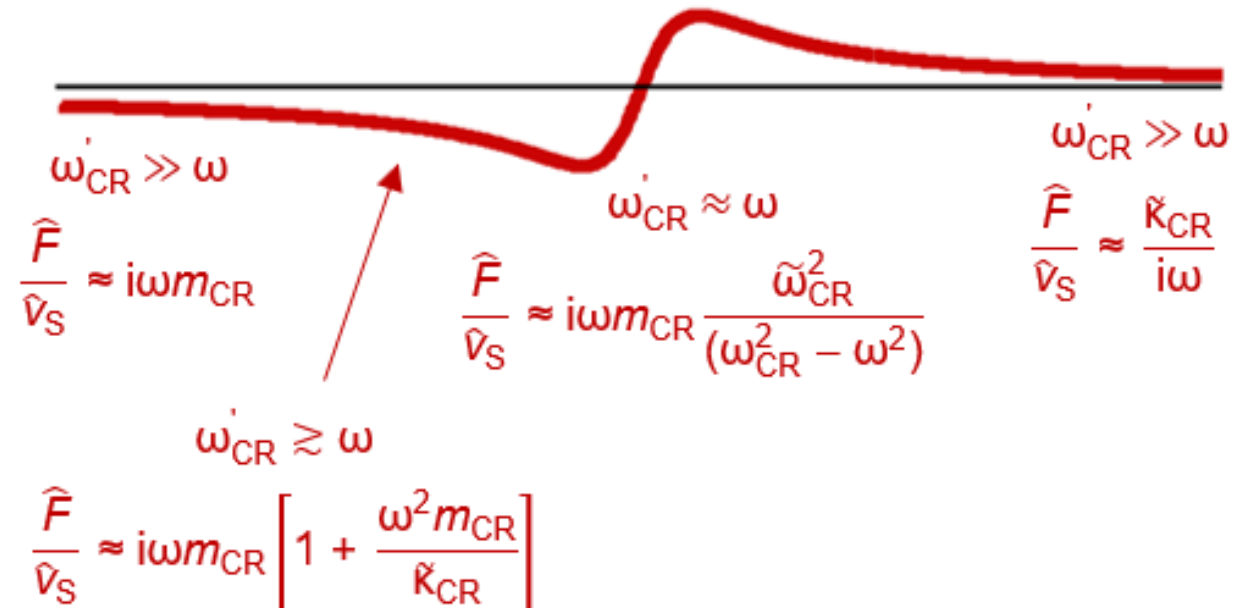
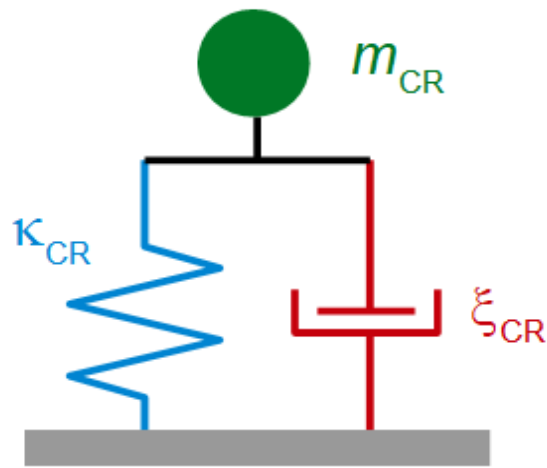
Viscoelastic parameters converted to $|G|$ and $\tan \delta_L$

Streptavidin



Particles, Coupled Resonances, Δf can be > 0

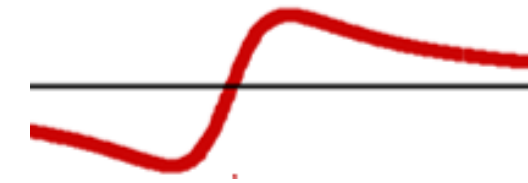
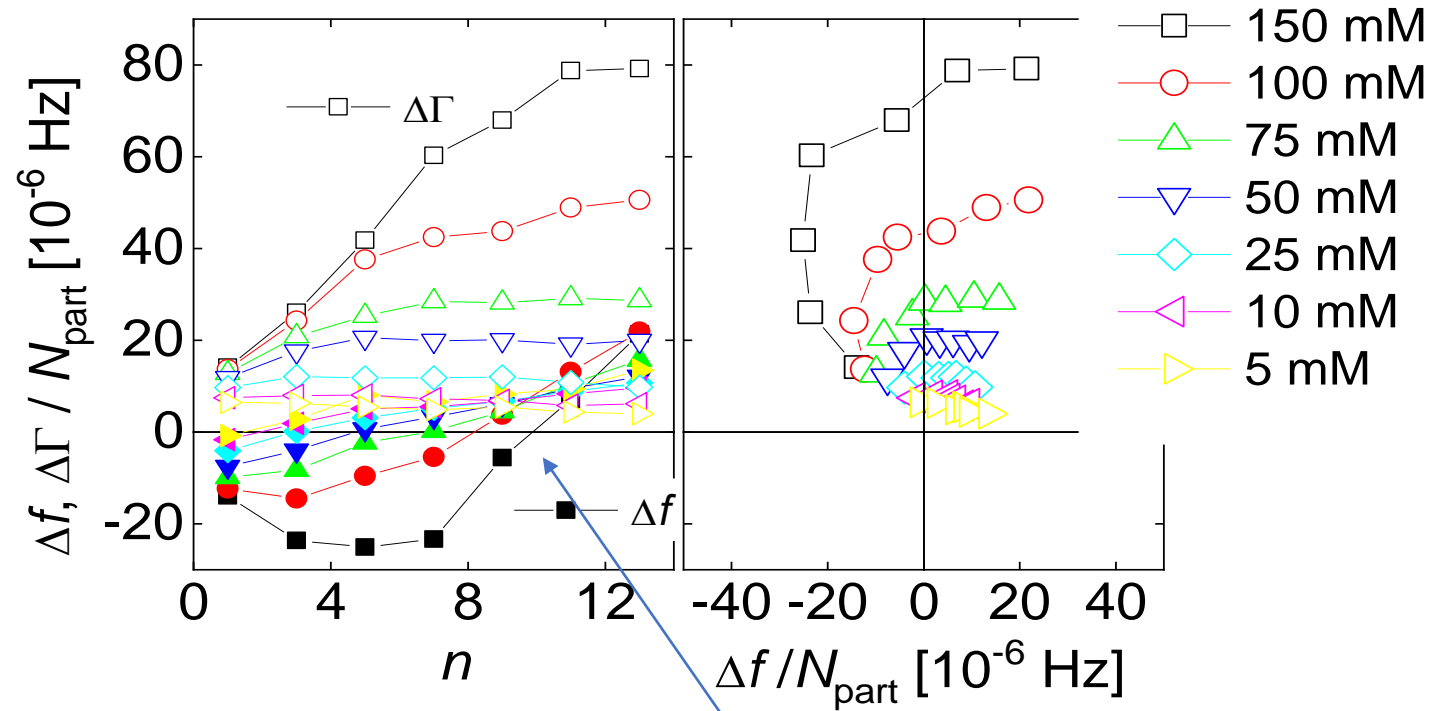
$$\frac{\Delta f + i\Delta\Gamma}{f_0} = -\frac{n_P}{A_{\text{eff}}} \frac{\omega m_{\text{CR}}}{\pi Z_q} \left[\frac{\tilde{\omega}_{\text{CR}}^2}{\tilde{\omega}_{\text{CR}}^2 - \omega^2} \right]$$



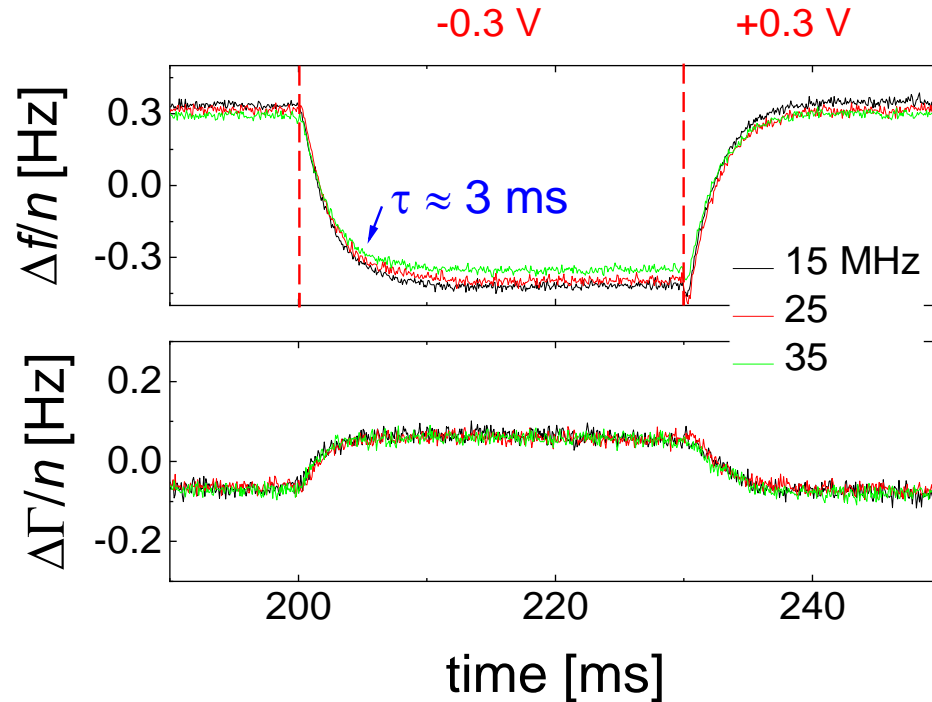
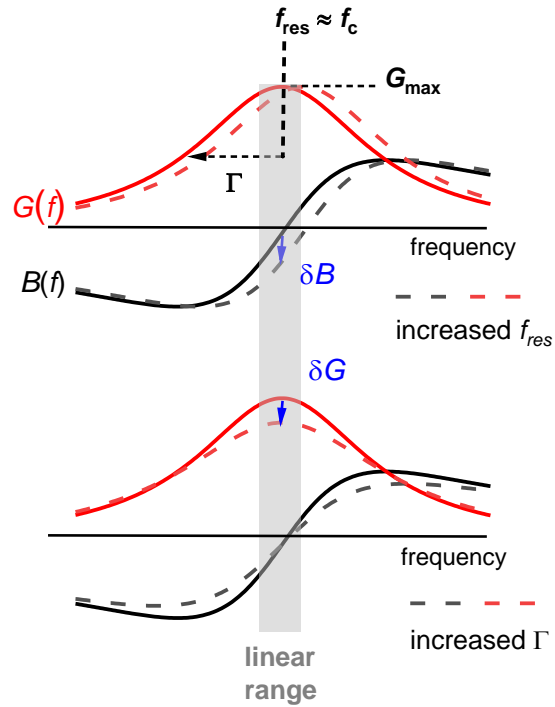
Coupled Resonances, $\Delta f > 0$

Shifts of frequency and bandwidth caused by the deposition of micron-sized silica spheres. The polar diagram on the right displays spirals, characteristic for the coupled resonance.

The ion strength as indicated in the legend tunes the stiffness of the contact, where large ion strength leads to stiff contacts.



Fast Measurements with the Fixed-Frequency-Drive Mode Application to the Electrochemical QCM (EQCM)



In this experiment, accumulation and averaging reduced the noise to a few mHz. This is the “**modulation QCM**”

- Leppin, C.; Peschel, A.; Meyer, F.; Langhoff, A.; Johannsmann, D. Kinetics of Viscoelasticity in the Electric Double Layer Studied by a Fast Electrochemical Quartz Crystal Microbalance (EQCM). *Analyst* 2021, 146, 2160–2171
- Pax, M.; Rieger, J.; Eibl, R.H.; Thielemann, C.; Johannsmann, D. Measurements of fast fluctuations of viscoelastic properties with the quartz crystal microbalance. *Analyst* 2005, 130, 1474–1477
- Montagut, Y.; Garcia, J.; Jimenez, Y.; March, C.; Montoya, A.; Arnau, A. Frequency-shift vs phase-shift characterization of in-liquid quartz crystal microbalance applications. *Rev. Sci. Instrum.* 2011, 82
- Guha, A.; Sandstrom, N.; Ostanin, V.; van der Wijngaart, W.; Klenerman, D.; Ghosh, S. Simple and ultrafast resonance frequency and dissipation shift measurements using a fixed frequency drive. *Actuators B-Chem.* 2018, 281, 960–970,

Conclusions

- The QCM-D gives access to thickness **and** softness
- It differentiates between **elastic** and **viscous** softness
- It can even do **viscoelastic spectroscopy** (“high frequency rheology”)
 - It can do so to some extent (one out of two **power-law exponents**)
- It’s an active field of research